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Relationships between physical capacities and biomechanical variables during movement tasks in athletic populations following anterior cruciate ligament reconstruction

32 **ABSTRACT**

33 **Background**

34 Anterior cruciate ligament (ACL) reconstruction has a detrimental impact on athletic
35 performance. Despite rehabilitation guidelines and criterion-based progressions to ensure safe
36 restoration of fundamental physical capacities and maladaptive movement strategies, residual
37 deficits in maximal strength, rate of force development (RFD), power and reactive strength
38 are commonly reported. These combined with associated compensatory inter and intra-limb
39 strategies increase the risk of re-injury.

40 **Objective**

41 The aim of this article is to examine the relationships between fundamental physical
42 capacities and biomechanical variables during dynamic movement tasks.

43 **Design**

44 Narrative review

45 **Results**

46 The available data suggests that quadriceps strength and rate of torque development, explain
47 a moderate portion of the variance in aberrant kinetic and kinematic strategies commonly
48 detected in ACL reconstructed cohorts at who are during the later stages of rehabilitation and
49 RTS

50 **Conclusion**

51 The available data suggests that quadriceps strength and rate of torque development, explain
52 a moderate portion of the variance in aberrant kinetic and kinematic strategies commonly
53 detected in ACL reconstructed cohorts at who are in the later stages of rehabilitation and RTS

54

55 **1. Introduction**

56 Sports such as soccer, basketball or rugby, require skills including pivoting, cutting, landing,
57 or jumping and expose athletes to a high risk (incidence rates from 0.03% to 3.67% per year)
58 of sustaining an anterior cruciate ligament (ACL) injury during their career (Lindanger,

59 Strand, Molster, Solheim, & Inderhaug, 2019; Moses, Orchard, & Orchard, 2012; Silvers-
60 Graneli, Bizzini, Arundale, Mandelbaum, & Snyder-Mackler, 2017). Following ACL
61 reconstruction, common return to sports (RTS) criteria are often achieved in cohorts with a
62 relatively low rate of return to competitive sport (Ardern, Webster, Taylor, & Feller, 2011;
63 Webster & Hewett, 2019). Thus, current approaches to determine physical capacity and
64 examine movement competency are considered in-adequate to identify those at a greater re-
65 injury risk (Losciale, Zdeb, Ledbetter, Reiman, & Sell, 2019). This may be partly linked to
66 biomechanical deficits which have been observed following ACL reconstruction, even in the
67 presence of normalized between-limb comparisons in measures such as hop distance (Davies,
68 Myer, & Read, 2019; Losciale, Bullock, et al., 2019), and change of direction times (King,
69 Richter, Franklyn-Miller, Daniels, Wadey, Jackson, et al., 2018).

70 Shallow knee flexion angle and pronounced knee valgus at the point of ground contact are
71 commonly cited as a mechanism of injury, corresponding with positions of peak ACL strain
72 (Della Villa, et al., 2020; Walden, et al., 2015). High magnitudes of knee joint loading,
73 expressed as knee abduction moment, are thought to reflect increased knee injury risk (Fox,
74 2018). Knee abduction moment is influenced by whole body biomechanics during jumping
75 and change of direction activities. In the ACL reconstructed limb, lower internal knee valgus
76 moment, knee internal rotation angle and ankle external rotation moment, with the centre of
77 mass less posterior to the knee are common findings across various single leg hop tests
78 (King, Richter, Franklyn-Miller, Daniels, Wadey, Moran, et al., 2018). In change of direction
79 activities typical features include, lateral flexion/rotation of the trunk and position of the
80 centre of mass away from the intended change of direction and from the stance leg, and
81 greater hip flexion and internal rotation at initial contact during cutting manoeuvres.
82 Furthermore, anticipatory adjustments in the step prior to penultimate foot contact during a
83 change of direction, can also alter kinetic and kinematic variables associated with ACL strain
84 magnitudes (Dos'Santos, Thomas, Comfort, & Jones, 2018).

85 Deficits in strength (Caroline Lisee, Lepley, Birchmeier, O'Hagan, & Kuenze, 2019;
86 Petersen, Taheri, Forkel, & Zantop, 2014), rate of force development (RFD) (Angelozzi, et
87 al., 2012; Davis, et al., 2017; Hsieh, Indelicato, Moser, Vandenborne, & Chmielewski, 2015;
88 Turpeinen, Freitas, Rubio-Arias, Jordan, & Aagaard), power (Castanharo, et al., 2011;
89 O'Malley, et al., 2018), and reactive strength (King, Richter, Franklyn-Miller, Daniels,
90 Wadey, Moran, et al., 2018; C. Lisee, Birchmeier, Yan, & Kuenze, 2019) have been
91 identified in different populations following ACL reconstruction. Therefore, rehabilitation

92 programmes have focused on regaining symmetrical range of motion and fundamental
93 physical capacities (i.e. strength, RFD, power, and reactive strength) (Buckthorpe & Della
94 Villa, 2019), in addition to normalisation of maladaptive biomechanical variables in a range
95 of dynamic tasks associated with high peak ACL strains and re-injury risk, such as jumping,
96 landing and change of direction (Gokeler, Neuhaus, Benjaminse, Grooms, & Baumeister,
97 2019). Nonetheless, the available data indicate that patients in the later stages of
98 rehabilitation and RTS following ACL reconstruction, exhibit maladaptive movement
99 strategies (i.e. altered neuromuscular control of the hip and knee during dynamic landing
100 tasks) that may expose them to a greater risk of re-injury (M. V. Paterno, et al., 2010). It is
101 currently unclear if these aberrant mechanics are underpinned by sub-optimal physical
102 capacities, graft type, time to RTS, psychological status or altered neuromuscular control.

103 Mounting body of evidence suggests that an adequate level of physical capacity is required to
104 facilitate the execution of more complex athletic skills (Cormie, McGuigan, & Newton,
105 2011a, 2011b). However, a synthesis of the literature to determine the extent to which deficits
106 in physical capacity affect biomechanical variables during movement execution in athletic
107 cohorts following ACL reconstruction is unclear. Therefore, the aim of this narrative review
108 was to examine relationships between strength, RFD, power, reactive strength, and kinetic
109 and kinematic variables in dynamic tasks in ACL reconstructed athletes in the later stages of
110 rehabilitation and RTS. The information included will assist clinicians, providing clear
111 practical applications to optimise RTS.

112 **2.0 Methodology**

113 The lead author conducted a literature search of three electronic databases (MEDLINE,
114 SPORTDiscus and CINHAL) on 5 March 2020. The studies were selected according to
115 PICOS framework (Participants, Intervention, Comparison, Outcome, and Study design)
116 (Liberati, et al., 2009). Cohort studies investigating strength, power, RFD or reactive
117 strength, and kinetic or kinematic variables in performance tests in participants at their later
118 stage rehabilitation and RTS following ACL reconstruction were considered. They had to be
119 published in peer-reviewed journals and written using English language not before 2010. The
120 keywords “strength” or “reactive strength” or “power” or “rate of force development” were
121 combined with the Boolean operator “AND” to keywords pertinent to kinetics, kinematics
122 and performance measures (e.g. “biomechanics”, “change of direction”, “landing”, etc.).

123 The additional inclusion criteria were: (1) participants with any graft type; (2) assessment of
124 strength, power, RFD, or reactive strength using dynamometers or force platforms; (3)
125 assessment of kinetic variables using force platforms; (4) assessment of kinematic variables
126 using 3D motion capture analysis.

127 **3.0 Physical capacity measurement**

128 In this next section we will briefly summarise the assessment modes of physical capacities
129 typically measured and described in ACL literature.

130 **3.1 Strength**

131 The majority of studies which have examined strength in athletic populations post ACL
132 reconstruction included an isokinetic dynamometer at a variety of test speeds
133 ($60^{\circ}/s$, $120^{\circ}/s$, $180^{\circ}/s$, and $300^{\circ}/s$) for both the quadriceps and hamstring muscles (Almeida,
134 Santos Silva, Pedrinelli, & Hernandez, 2018; Baltaci, Yilmaz, & Atay, 2012; Królikowska,
135 Reichert, Czamara, & Krzemińska, 2019; Miles & King, 2019; Mohammadi, et al., 2013;
136 O'Malley, et al., 2018; Welling, Benjaminse, Lemmink, Dingenen, & Gokeler, 2019; Xergia,
137 Pappas, Zampeli, Georgiou, & Georgoulis, 2013). Other testing modes included isometric
138 MVIC on a dynamometer (Holsgaard-Larsen, Jensen, Mortensen, & Aagaard, 2014; Norouzi,
139 Esfandiarpour, Mehdizadeh, Yousefzadeh, & Parnianpour, 2019; Schmitt, Paterno, Ford,
140 Myer, & Hewett, 2015; Timmins, et al., 2016; Ward, et al., 2018), or uniaxial load cells
141 (Timmins, et al., 2016).

142 **3.2 Power**

143 The product of force (or strength) and velocity results in mechanical power; which, when
144 divided by time, defines the rate at which work is performed (Turner, et al., 9000). The
145 ability to express high power outputs is an important factor related to increasing performance
146 levels (Haff & Stone, 2015). Given the components of power (P), it appears intuitive that
147 strength (indicating high levels of force production) and speed are the main physical
148 determinants of athletic skills, such as jumping, landing (given the need for braking force),
149 accelerating, and changing direction (Haff & Stone, 2015; Turner, et al., 9000). In ACL
150 literature power has been calculated primarily during bilateral (Castanharo, et al., 2011;
151 Read, Michael Auliffe, Wilson, & Graham-Smith, 2020) and single countermovement jumps
152 (CMJ) (O'Malley, et al., 2018). The synchronisation of kinetic and kinematic data has also
153 been used to assess single joint power contribution, highlighting intra-limb compensation

154 strategies commonly documented in ACL reconstructed cohorts (Baumgart, Schubert, Hoppe,
155 Gokeler, & Freiwald, 2017; Gokeler, et al., 2010; M. V. Paterno, Ford, Myer, Heyl, &
156 Hewett, 2007).

157 **3.3 Rate of force development (RFD)**

158 RFD is defined as the ability of the neuromuscular system to produce a high rate in the rise of
159 muscle force in the first 30-250 milliseconds (Taber, Bellon, Abbott, & Bingham, 2016), and
160 it is calculated as $\Delta\text{Force}/\Delta\text{Time}$, which is determined from the slope of the force time curve
161 (generally between 0 and 250 milliseconds) (Maffiuletti, et al., 2016; Rodriguez-Rosell,
162 Pareja-Blanco, Aagaard, & Gonzalez-Badillo, 2018). Impaired knee extension rate of torque
163 development has been reported following ACL reconstruction (Angelozzi, et al., 2012; Pua,
164 Mentiplay, Clark, & Ho, 2017; Turpeinen, et al.). Assessment of RFD in a dynamic task (i.e.
165 CMJ) has only been recently investigated (Read, et al., 2020). Preliminary findings showed
166 significant differences in eccentric deceleration RFD asymmetry between ACL reconstructed
167 participants and healthy controls (Read, et al., 2020), even greater than 9 months post-surgery
168 which warrants further investigation to examine its validity to detect rehabilitation status and
169 readiness to RTS (Read, et al., 2020).

170 **3.4 Reactive Strength**

171 Specific qualities of strength, such as maximal eccentric strength, underpin an athlete's
172 reactive-strength ability, allowing efficient storage and reutilisation of elastic energy during
173 stretch-shortening cycle activities (Beattie, Carson, Lyons, & Kenny, 2017; Suchomel, et al.,
174 2019). Quantification is typically via reactive strength index (RSI) = jump height (m) /
175 ground contact time (sec) during a drop vertical jump (DVJ) task (Flanagan & Comyns,
176 2008).

177 Reactive strength has been assessed in ACL reconstructed cohorts during a single leg drop
178 jump (SLDJ) (King, Richter, Franklyn-Miller, Daniels, Wadey, Moran, et al., 2018; C. Lisee,
179 et al., 2019). In their cohort of 156 male multidirectional sports athletes, King et al., (King,
180 Richter, Franklyn-Miller, Daniels, Wadey, Moran, et al., 2018) found significant inter-limb
181 asymmetries in RSI (21% deficits in the ACLR side, $d = 0.73$). This may have important
182 clinical implications given that reactive strength significantly correlate with a reduced
183 metabolic cost of running (running economy at 12-16 km·h⁻¹) and change of direction

184 performance (Li, Newton, Shi, Sutton, & Ding, 2019; Maloney, Richards, Nixon, Harvey, &
185 Fletcher, 2017).

186 **4.0 Movement tasks assessed**

187 Bilateral jumping and landing tasks provide valuable insights on underlying kinematic and
188 kinetic strategy. Single leg jumping, and landing tasks increase the load that the single limb
189 needs to withstand, with speculation that single leg dynamic tasks better reflect a measure of
190 limb capacity (Cohen, et al. 2020). However, bilateral jumping assessments such as the CMJ
191 or DVJ, offer more options to unload the ACL reconstructed limb than single leg tasks. This
192 may occur via inter-limb compensatory strategies in which the uninjured limb is favoured,
193 off-loading the previously injured side (Baumgart, et al., 2017; Dai, Butler, Garrett, & Queen,
194 2014; Hart, et al., 2019). This can be easily quantified by the vertical ground reaction force
195 (vGRF) generated. Furthermore, force platform assessment of CMJ performance allows
196 identification of phase specific vGRF (eccentric, concentric and landing phase variables) as
197 well as the time to complete these phases (Hart, et al., 2019).

198 Intra-limb compensation strategies may also be adopted in which lower peak power
199 generation at the knee is compensated for by a higher proportion of power at proximal or
200 distal joints (i.e. hip or ankle). These asymmetries appeared evident in sagittal plane variables
201 such as hip extension moments ($d=0.60$) during the eccentric phase, and hip flexion angles
202 ($d=0.57$) and ankle plantar-flexion moments ($d=0.59$) at the end of the stance phase during
203 DVJ push-off (King, et al., 2019). More pronounced inter-limb asymmetries were also
204 evident in the frontal and transverse planes for internal knee valgus moment ($d=0.5$) and
205 ankle external rotation moment ($d=0.51$) through the middle of the stance phase in ACL
206 reconstructed athletes vs. healthy controls (King, et al., 2019).

207

208 **5.0 Relationship between strength and kinetic variables**

209 Schmitt et al. (Schmitt, et al., 2015) assessed quadriceps MVIC with an isokinetic
210 dynamometer at 60° knee flexion in relatively young participants (n=77, mean age=17 years)
211 who completed their rehabilitation programme and were cleared to return to high-level
212 athletic activities (cutting and pivoting). They found significant correlations between
213 quadriceps index (involved / un-involved x 100) and kinetic variables in the bilateral DVJ
214 from a 31 cm box. No kinetic differences were reported between participants displaying high

215 quadriceps index (>90%) and matched controls for any limb symmetry measures. Those with
216 low quadriceps index (<85%) demonstrated greater limb asymmetry in sagittal plane knee
217 joint mechanics (i.e. peak external knee flexion moment ($p<0.001$), peak vGRF ($p<0.001$)
218 and peak loading rate ($p=0.008$) during the landing phase compared to the stronger
219 individuals. Quadriceps index was the only significant predictor (beta value= .412; $p<0.001$)
220 for limb symmetry index (LSI) peak vGRF ($R^2= .274$) and for LSI loading rate ($R^2= .152$,
221 beta value= .253; $p=0.04$) after controlling for graft type, presence of meniscus injury, knee
222 pain, and knee symptoms. For LSI, peak external knee flexion moment ($R^2= .501$), graft type
223 (beta value=0.295, $p=0.002$) and quadriceps index (beta value=0.510, $p<0.001$) were the only
224 statistically significant predictors. Ward et al. (Ward, et al., 2018) also observed a low
225 negative association between MVIC and peak vGRF ($r= -0.41$, $R^2= .17$, $p=0.03$) measured
226 during a DVJ, indicating that greater knee extension strength may minimise vGRF, although
227 only a small amount of the variance in kinetic strategies was explained. In female athletes,
228 lower vGRF on the ACLR limb compared to the uninvolved limb may also be present 2 years
229 post-surgery in both the landing and takeoff phase of a DVJ (M. V. Paterno, et al., 2007).
230 This strategy has been associated with increased risk of ACL injury in female athletes
231 (Hewett, et al., 2005), and has also been documented in mixed populations (Baumgart, et al.,
232 2017; King, Richter, Franklyn-Miller, Daniels, Wadey, Moran, et al., 2018; Mark V. Paterno,
233 et al., 2011).

234 Quadriceps strength also appears to effect slower movements as well as rebound tasks, as
235 Miles et al. (Miles & King, 2019) observed a relationship between quadriceps strength and
236 kinetics during a CMJ. Knee extensor strength asymmetry explained 39% ($R^2= .39$; $p=0.002$)
237 and 18% ($R^2= .18$; $p=0.04$) of the variation in concentric impulse asymmetry during the CMJ
238 in the bone patella tendon bone and the semitendinosus/gracilis groups respectively. No
239 significant relationship was shown between knee extensor strength asymmetry and eccentric
240 impulse asymmetry in any group. Thus, targeted strategies to increase quadriceps strength
241 appear warranted to improve aberrant kinetics during bilateral tasks.

242 Strength also appears to be related to kinetic parameters during single leg jumping. In young
243 athletes cleared to return to high-level athletic activities (cutting and pivoting) following
244 ACL reconstruction (Ithurburn, Paterno, Ford, Hewett, & Schmitt, 2015; Palmieri-Smith &
245 Lepley, 2015), greater kinetic asymmetries during a single leg horizontal (Palmieri-Smith &
246 Lepley, 2015) and vertical (Ithurburn, et al., 2015) landing task were more pronounced in
247 participants with low quadriceps index compared to those with higher symmetry scores.

248 Similarly, 78% of the variability in the lower external knee flexion moment detected in the
249 ACL reconstructed limb during a single leg landing was explained by the knee extensor
250 muscular capacities ($R^2 = .78$; $p < 0.002$) (Oberländer, Brügemann, Höher, &
251 Karamanidis, 2013). In the work of Palmieri-Smith et al. (Palmieri-Smith & Lepley, 2015),
252 for knee flexion moment symmetry, only age ($p = 0.042$) and quadriceps index ($p = 0.008$) were
253 significant predictors (R^2 change = 0.250 for quadriceps index) after controlling for age, mass,
254 gender, time to RTS and meniscal status. Peak knee extension moment symmetry in the
255 vertical drop land task was significantly predicted by quadriceps index (R^2 adjusted = .102;
256 $p < 0.001$) (Ithurnburn, et al., 2015).

257 O'Malley et al. (O'Malley, et al., 2018) found inter-limb differences in ACL reconstructed
258 athletes in isokinetic knee-extension peak torque ($d = -1.33$), isokinetic knee-flexion peak
259 torque ($d = -0.19$) single leg CMJ hip power contribution ($d = 0.75$), peak power ($d = -0.47$),
260 and knee power contribution ($d = -0.37$). Low to moderate correlations ($r = 0.28-0.31$) were
261 also reported between isokinetic knee extension peak torque and power generation at each
262 joint in the single leg CMJ. These data reinforce the notion that in unilateral tasks such, the
263 ACL reconstructed limb may adopt intra-limb compensation strategies for lower peak power
264 generation at the knee by generating a higher proportion of power at the hip. This is further
265 evident as isokinetic knee extensor peak torque could only explain a small amount of
266 variance in peak power generation during a single leg CMJ (O'Malley, et al., 2018). To our
267 knowledge, the relationship between single leg DVJ kinetic parameters and strength levels in
268 ACL reconstructed cohorts has not been examined and further research is warranted. Indeed,
269 evident compensatory strategies following ACL reconstruction include reduced ability to
270 absorb and regenerate ground reaction forces upon landing (Lloyd, Oliver, Kember, Myer, &
271 Read, 2020).

272

273 **5.1 Relationship between strength and kinematic variables**

274 Three dimensional kinematic data were collected using camera motion-systems and retro-
275 reflective markers across different studies (Gokeler, et al., 2010; Ithurnburn, et al., 2015; C.
276 Lisee, et al., 2019; Oberländer, et al., 2013; Palmieri-Smith & Lepley, 2015; Schmitt, et al.,
277 2015; Ward, et al., 2018). During a bilateral DVJ from a 31 cm box, Ward et al. (Ward, et al.,
278 2018) observed lower knee-flexion angles at initial contact ($p = 0.03$) in the ACL
279 reconstructed limb, whereas Schmitt et al. (Schmitt, et al., 2015) did not find any significant

280 between-limb kinematic difference. A low positive association was reported between knee
281 extensor MVIC and peak knee flexion angle ($r = 0.38$, $R^2 = 0.14$, $p = 0.045$) (Ward, et al.,
282 2018). Due to the paucity of studies which have examined the relationship between strength
283 and kinematic variables in bilateral dynamic tasks, further research is warranted.

284 Equally, only a few studies have measured associations between physical capacities and
285 kinematic variables in unilateral dynamic tasks. Compared to matched controls, greater limb
286 asymmetry during a single leg drop landing task in knee flexion excursion and peak trunk
287 flexion angle was found in ACL reconstructed participants cleared to return to high-level
288 athletic activities (cutting and pivoting) (Ithurnburn, et al., 2015). Compared to the
289 contralateral limb, decreased knee flexion excursion (Gokeler, et al., 2010; Ithurnburn, et al.,
290 2015; Palmieri-Smith & Lepley, 2015) and increased peak trunk flexion angle was reported
291 (Ithurnburn, et al., 2015; OberlÄNder, et al., 2013). These asymmetries during landing were
292 more pronounced in participants with low quadriceps index compared to those displaying
293 greater symmetry. Peak trunk flexion and knee flexion excursion symmetry were
294 significantly predicted by quadriceps index (R^2 adjusted= .153, $p < 0.002$ and R^2 adjusted=
295 .116, $p < 0.001$ respectively) (Ithurnburn, et al., 2015). This suggests that participants with low
296 quadriceps index following ACLR adopt a strategy of greater trunk flexion when landing on
297 the ACL reconstructed limb in a single leg drop landing task possibly to compensate for
298 decreased knee extension strength. Similarly, in a predominantly female ACL reconstructed
299 population, peak knee flexion angle during a single leg drop crossover hop task was predicted
300 by peak knee extension torque ($R^2 = .467$, beta value= 8.517; $p < 0.001$) (C. Lisee, et al., 2019),
301 but this had no predictive value for any kinematic variable in the single leg step down task.

302 Collectively, the available evidence suggests that: 1) the level of correlation between knee
303 extensor and flexor strength and kinematic variables needs to be further examined in relation
304 to gender and task; 2) ACL reconstructed participants tend to adopt a “stiffer” landing
305 strategy in the affected knee with less knee ROM during landing; 3) greater trunk flexion
306 when landing in the single leg drop landing task on the injured limb may be adopted to
307 compensate for decreased knee extension strength; 4) knee extensor deficits explain only a
308 part of the variance in peak knee and trunk flexion angle in unilateral and bilateral tasks.

309 **6.0 Correlation between RFD/power, kinetic and kinematic variables**

310 Emerging research (Read, et al., 2020) showed that the involved limb of male adults
311 following ACL reconstruction (> 6 months post-surgery) displays significantly lower

312 eccentric deceleration RFD during a CMJ compared to the uninvolved limb. While in healthy
313 individuals, positive correlations between knee extension RTD and jump performance have
314 been indicated (Chang, Norcross, Johnson, Kitagawa, & Hoffman, 2015; de Ruiter, Van
315 Leeuwen, Heijblom, Bobbert, & de Haan, 2006; de Ruiter, Vermeulen, Toussaint, & de
316 Haan, 2007), the extent of this association with biomechanical variables in ACL
317 reconstructed participants is currently lacking.

318 Castanharo et al. (Castanharo, et al., 2011) compared CMJ performance and kinetic variables
319 between a group of ACL reconstructed adult males with semitendinosus/gracilis graft ≥ 2
320 years post-surgery and a control group. No significant differences in jump height were
321 present between groups, but peak knee joint power on the injured side was 13% lower than
322 the contralateral limb. These results highlight an “offloading” strategy of the involved limb.
323 These results are in line with a recent systematic review and meta-analysis (Kotsifaki,
324 Korakakis, Whiteley, Van Rossom, & Jonkers, 2019), which showed moderate evidence of a
325 strong effect for lower power absorption in the reconstructed knee ($d = -0.98$, 95% CI -1.37
326 to -0.60) during the SL hop.

327 Read et al. (Read, et al., 2020) observed that despite obtaining similar jump height in the
328 CMJ, the ACL reconstructed group at 6-9 months post-surgery displayed significantly greater
329 asymmetry indexes in concentric impulse (9.6 ± 5.6 ; 95% CI: 8.2-10.9) and concentric peak
330 vGRF (8.0 ± 4.3 ; 95% CI: 6.9-9.0) than the ACL reconstructed group at >9 months post-
331 surgery (7.4 ± 5.1 ; 95%: CI 6.0-8.8, and 6.6 ± 4.2 ; 95%: CI 5.5-7.7). No significant
332 differences between ACL reconstructed groups in asymmetry indexes were found in eccentric
333 deceleration impulse and peak landing vGRF. However, asymmetry of all the aforementioned
334 kinetic variables were greater in the involved limb of the ACL reconstructed participants than
335 in the dominant limb of healthy controls with effect sizes ranging from moderate to very
336 large ($d = 0.54$ - 1.35).

337 These results are in line with recent research (Jordan, Aagaard, & Herzog, 2018; Miles &
338 King, 2019), which showed greater concentric impulse asymmetry in ACL reconstructed
339 participants compared to healthy controls during bilateral jumping tasks. These residual
340 deficits indicate inter-limb strategies that redistribute impulse production to favour the
341 uninvolved side. Also, concentric impulse asymmetry index was strongly associated with
342 rehabilitation status ($p < 0.001$). Furthermore, similar to Mohammadi et al. (Mohammadi, et

343 al., 2013) concentric peak vGRF were reduced on the ACL reconstructed side, thus indicating
344 compensatory strategies which offload the involved limb in dynamic tasks.

345 During unilateral jumping, O'Malley et al. (O'Malley, et al., 2018) found inter-limb
346 differences in the ACL reconstructed group in single leg CMJ hip power contribution (d
347 =0.75), jump height ($d = -0.71$), peak power ($d = -0.47$), and knee power contribution ($d = -$
348 0.37). Similar differences were also found between groups in jump height LSI ($d = -1.12$),
349 jump height ($d = -0.86$), peak power LSI_{modified} ($d = -0.61$), hip power contribution ($d =$
350 0.61), and knee power contribution ($d = -0.40$). This reinforces the notion that in unilateral
351 tasks, the ACL reconstructed limb may adopt intra-limb compensation strategies for lower
352 peak power generation at the knee by generating a higher proportion of power at the hip and
353 ankle.

354 A recent study also analysed knee extensor early (<100ms) and late RTD (>100ms) and their
355 association with performance tests in ACL reconstructed athletes. Birchmeier et al.
356 (Birchmeier, Lisee, Geers, & Kuenze, 2019) showed that both RTD₁₀₀ and RTD₂₀₀ had no
357 significant correlation with amortization time in the single leg DVJ, but were moderately
358 correlated with jump height ($r= 0.391$ and 0.473 respectively). Lisee et al. (C. Lisee, et al.,
359 2019) revealed that only RTD₂₀₀ had a weak relationship with peak knee extension moment
360 ($R^2= .176$, beta value= 0.066 ; $p<0.025$) in a single leg step down task. Together, the data
361 suggests that the ability of the quadriceps to generate force rapidly may be important for
362 lower extremity loading characteristics in hopping and jumping.

363 There is a paucity of studies to examine RFD/power and kinematic variables in this cohort.
364 Lisee et al. (C. Lisee, et al., 2019) showed that after ACL reconstruction, females with poorer
365 quadriceps RFD₁₀₀ landed with smaller knee flexion angles at initial contact during a single
366 leg drop crossover hop task ($R^2= .198$, beta value= 0.721 ; $p<0.013$). Further studies are
367 needed to investigate associations between RFD and kinematic variables in performance tests
368 following ACL reconstruction.

369

370 **7.0 Relationship between reactive strength and kinetic and kinematic variables**

371 King et al. (King, Richter, Franklyn-Miller, Daniels, Wadey, Moran, et al., 2018) examined
372 RSI and kinetic variables in performance tests in an ACL reconstructed adult male population
373 involved in multidirectional sports approximately at 9 months post-surgery (n=156, mean age

374 24.8 ± 4.8). They showed reduced RSI (21% deficit) in the injured compared to the
375 contralateral limb ($d = -0.73$). However, no analysis was completed to identify the
376 predictive role of RSI on kinetic variables. To our knowledge, only Birchmeier et al.
377 (Birchmeier, et al., 2019) assessed the extent of the association between RSI and kinetic
378 variables in a mixed cohort. No significant correlation was reported between RSI and
379 amortization time in single leg DVJ. Significant correlations were found between RSI and
380 triple hop distance ($r= 0.689$) and SLDJ height ($r=0.609$) (Birchmeier, et al., 2019). These
381 findings may appear logical considering that RSI is a measure of stretch-shortening cycle
382 performance, hence higher scores in RSI would positively enhance performance in repetitive
383 jumps. Further research should explore if RSI values are predictive of relevant kinematic
384 variables in participants following ACL reconstruction during rebound tasks.

385 A summary of the included studies investigating the relationship between physical capacities
386 and biomechanical variables during dynamic tasks in ACL reconstructed individuals is

387 included in Table 1. Figure 1 depicts kinetic and kinematic variables commonly found in ACL reconstructed cohorts during the DVJ and
 388 SLDVJ.

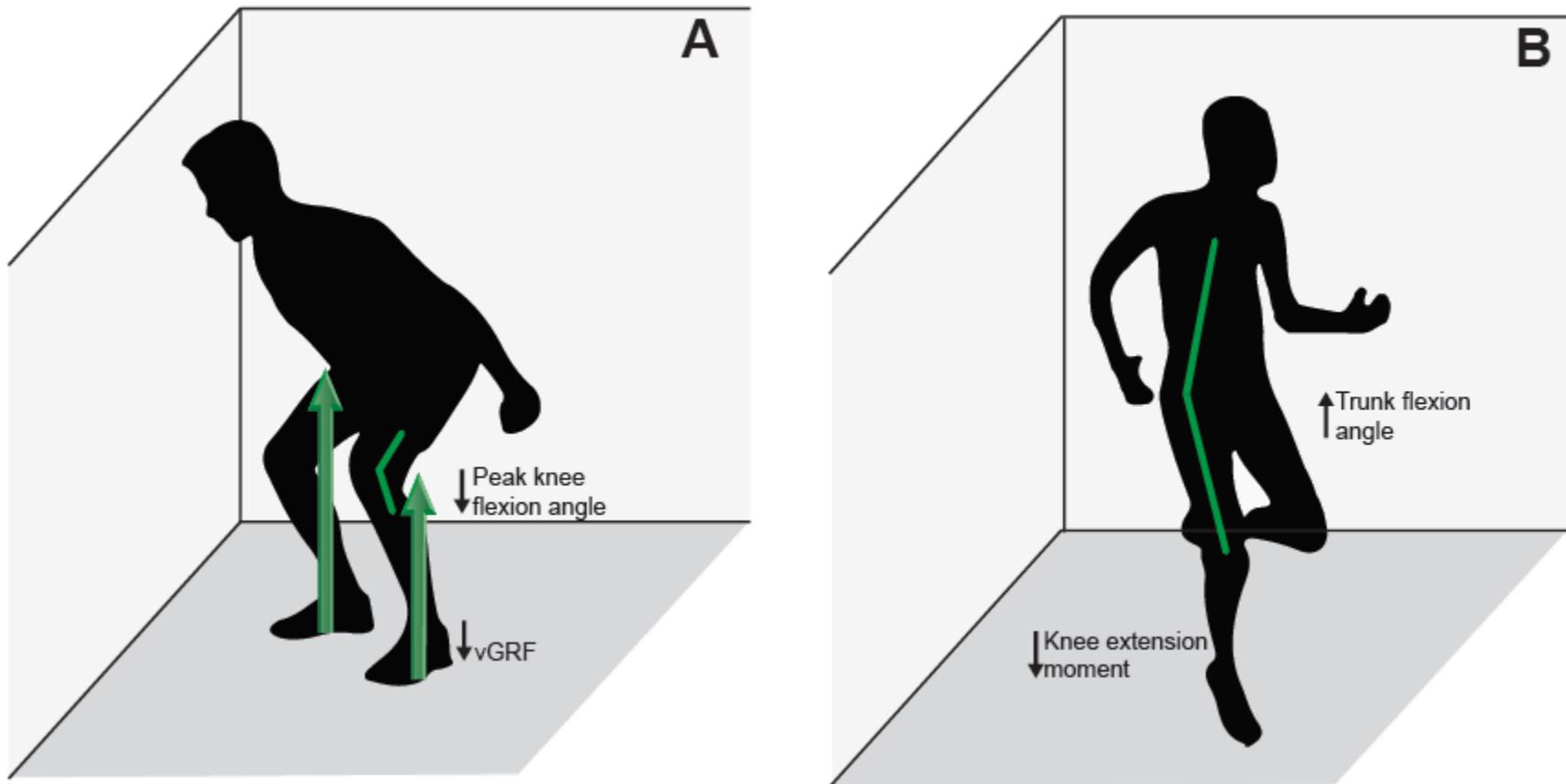
AUTHOR AND YEAR	PARTICIPANTS AND AGE (years)	PHYSICAL CAPACITIES TESTED	DYNAMIC TASK	MAIN FINDINGS
Schmitt (2015)	77 (males and females) Between 14 and 25	Knee extension isometric strength (MVIC) with an isokinetic dynamometer	DL DVJ Participants were positioned on the top of a 31-cm box and were instructed to drop off the box simultaneously with both feet, landing with each foot onto separate force platforms and then to perform a maximal effort vertical jump	<p style="text-align: center;">KINETIC</p> <p>Quadriceps index was the only significant predictor (beta value= .412; $p < 0.001$) for limb symmetry index (LSI) peak vGRF ($R^2 = .274$) and for LSI loading rate ($R^2 = .152$, beta value= .253; $p = 0.04$) after controlling for graft type, presence of meniscus injury, knee pain, and knee symptoms. For LSI, peak external knee flexion moment ($R^2 = .501$), graft type (beta value=0.295, $p = 0.002$) and quadriceps index (beta value=0.510, $p < 0.001$) were the only statistically significant predictors</p> <p style="text-align: center;">KINEMATIC</p> <p>No significant between-limb kinematic difference</p>
Ward (2018)	28 (males and females) 22.4 ± 3.7	Knee extension isometric strength (MVIC) with a dynamometer	DL DVJ Participants performed a jump-landing task from a 30-cm box positioned at 50% of the participant's height from the front edge of the force plates. They jumped forward off the box to a double-legged landing with 1 foot on each force plate and then immediately jumped vertically as high as possible	<p style="text-align: center;">KINETIC</p> <p>Low negative association between MVIC and peak vGRF ($r = -0.41$, $R^2 = 0.17$, $p = 0.03$)</p> <p style="text-align: center;">KINEMATIC</p> <p>Low positive association was reported between knee extensor MVIC and peak knee flexion angle ($r = 0.38$, $R^2 = 0.14$, $p = 0.045$)</p>

<p>Miles (2019)</p>	<p>Males only</p> <p>44 = 22BPTB + 22STG</p> <p>BPTB 23.4 ± 4.4 STG 26.1 ± 4.4</p>	<p>Isokinetic concentric knee extension and flexion strength (60°/s)</p>	<p>DL CMJ</p> <p>Participants were instructed to maintain hands placed on iliac crests and to jump as high as they could with knees extended during the flight phase</p>	<p>KINETIC</p> <p>Knee extensor strength asymmetry explained 39% ($R^2 = .39$; $p=0.002$) and 18% ($R^2 = .18$; $p=0.04$) of the variation in concentric impulse asymmetry during the CMJ in the bone patella tendon bone (BPTB) and the semitendinosus/gracilis (STG) groups respectively.</p> <p>No significant relationship was shown between knee extensor strength asymmetry and eccentric impulse asymmetry in any group</p>
<p>Ithurburn (2015)</p>	<p>103 (males and females)</p> <p>17.4</p>	<p>Knee extension isometric strength (MVIC) with an isokinetic dynamometer</p>	<p>SL drop land</p> <p>Participants stood at the edge of a 31-cm box on the limb being tested and were instructed to drop off of the box and land on a force platform on the same limb. Participants were required to maintain a controlled landing for at least 3 seconds after landing</p>	<p>KINETIC</p> <p>Quadriceps index was a significant predictor of peak knee extension moment LSI (R^2 adjusted = .102; $p<0.001$)</p> <p>KINEMATIC</p> <p>Quadriceps index was a significant predictor of knee flexion excursion LSI (R^2 adjusted = .116; $p<0.001$) and peak trunk flexion angle LSI (R^2 adjusted = .153; $p<0.001$)</p>
<p>Palmieri-Smith (2015)</p>	<p>66 (males and females)</p> <p>14-30</p>	<p>Isokinetic concentric knee extension strength (60°/s)</p>	<p>SL hop</p> <p>Participants stood on their test leg and hopped forward as far as possible landing only on the same leg</p>	<p>KINETIC</p> <p>For knee flexion moment symmetry, only age ($p=0.042$) and quadriceps index ($p=0.008$) were significant predictors (R^2 change= 0.250 for quadriceps index) after controlling for age, mass, gender, time to RTS and meniscal status. Peak knee extension moment symmetry in the vertical drop land task was significantly predicted by quadriceps index (R^2 adjusted= .102; $p<0.001$)</p> <p>KINEMATIC</p> <p>Meniscal status, mass, and time to return to activity were not found</p>

				to be significant predictors of biomechanical symmetry for peak knee flexion angle ($p > 0.05$), while age ($p = 0.013$) and gender ($p = 0.049$) did influence values. After controlling for all these variables in the model quadriceps index was also a significant predictor for knee flexion angle symmetry (R^2 change = .285)
Oberlander (2013)	10 (gender not specified) 28 ± 7	Isometric strength (MVIC) with a custom-built dynamometer with a strain gauge load cell	SL hop test Participants performed a modified single leg hop test for distance, keeping their hands on their hips. This hop was performed with one leg over a given distance of 0.75 x body height. Landing had to be on the force plate within a target area corresponding to the given distance ± 5 cm.	KINETIC 78% of the variability in the lower external knee flexion moment detected in the ACLR limb was explained by the knee extensor muscular strength ($R^2 = .78$; $p < 0.002$)
O'Malley (2018)	Males only 118 Patellar tendon 23.6 ± 5.8	Isokinetic concentric knee extension and flexion strength ($60^\circ/s$)	SL CMJ Participants were instructed to stand with 1 foot on the force plate and the free leg behind at approximately 90° . With their hands on their iliac crests, they were asked to complete an SL CMJ, jumping as high as possible.	KINETIC Low to moderate correlations ($r = 0.28-0.31$) were reported between isokinetic knee extension peak torque and power generation at each joint
Lisee (2019)	52 (males and females)	Knee extension isometric strength (MVIC) and RTD with an isokinetic dynamometer	SL step down Participants were instructed to step down off a 30-cm box onto the force plate and	KINETIC Peak knee extension torque is the only predictor of peak knee extension moment ($R^2 = .404$) during SL drop crossover hop landing. RTD200 had a weak relationship with peak knee extension moment

	22.6 ± 4.4		<p>continue walking forward as if stepping off the final step of a set of stairs.</p> <p>SL drop crossover hop Participants were instructed to jump off the involved limb from a 30 cm box landing onto the force plate with the same limb. Immediately after landing on the force plate, participants hopped as far as possible diagonally along a line projecting 45° from the center of the force plate</p>	<p>(R²= .176, beta value= 0.066; <i>p</i><0.025) during the SL step down</p> <p>KINEMATIC Peak knee flexion angle was predicted by peak knee extension torque (R²= .467, beta value= 8.517; <i>p</i><0.001)) Individuals with poorer quadriceps RFD100 landed with smaller knee flexion angles at initial contact (R²= .198, beta value= 0.721; <i>p</i><0.013) during SL drop crossover hop landing</p>
Birchmeier (2019)	<p>52 (males and females)</p> <p>22.9 ± 5.0</p>	<p>Knee extension isometric strength (MVIC) and RTD with an isokinetic dynamometer</p> <p>RSI measured during a SLDVJ</p>	<p>SL hop Participants hopped as far as possible from the designated starting line on one leg</p> <p>SL triple hop for distance Participant hopped 3 consecutive times on the same leg as far as possible</p>	<p>KINETIC Peak knee extension torque, RTD100 and RTD200 had no significant correlation with amortization time in the SLDJ</p>

389 **Table 1** Summary of the included studies investigating the relationship between physical capacities and biomechanical variables during dynamic
390 tasks in ACL reconstructed individuals



391

392 **Figure 1** Example of kinetic and kinematic variables commonly found in ACL reconstructed cohorts during the (A) drop vertical jump (DVJ)
393 and (B) single leg drop vertical jump (SLDVJ)

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395

396 **8.0 Practical applications and recommendations for future research**

397 Deficits in knee extensor torque are commonly reported in ACL reconstructed cohorts and are associated with inter-limb and intra-limb
398 compensation strategies indicative of greater re-injury risk (Ithurburn, et al., 2015; C. Lisee, et al., 2019; Miles & King, 2019; O'Malley, et al.,
399 2018; OberlÄNder, et al., 2013; M. V. Paterno, et al., 2007; M. V. Paterno, et al., 2010; Schmitt, et al., 2015). Specifically, in bilateral tasks
400 inter-limb compensation strategies are adopted to reduce GRF on the ACL reconstructed limb, whereas in unilateral tasks intra-limb
401 “offloading” strategies reduce the peak vGRF and power contribution at the knee by generating more power at the hip and ankle joint. Knee
402 extensor strength deficits explain part of the variance in kinematic variables such as peak knee ($R^2=14\%$ to 46.7%) and trunk flexion angles, and
403 in kinetic variables such as, peak knee extension moment ($R^2= 40.4\%$ to 78%), peak vGRF ($R^2=17\%$ to 27.4%) and concentric impulse
404 asymmetry ($R^2=18\%$ to 39%) in jumping tasks. Concentric impulse asymmetry index during a CMJ is strongly associated with rehabilitation
405 status, with lower values indicating better function (Miles & King, 2019) and is related to quadriceps strength [8]. Therefore, it appears of the
406 utmost importance that strategies to increase maximal quadriceps strength are an integral component of rehabilitation. Large deficits in peak
407 knee extension strength are commonly reported in ACL reconstructed participants at the later stages of rehabilitation and RTS (Johnston,
408 McClelland, Feller, & Webster, 2020; Maestroni, Read, Turner, Korakakis, & Papadopoulos, 2021). Thus, sports and healthcare professionals
409 are encouraged to adopt specific exercise selection, dosage and progressions in line with current best practice ("American College of Sports
410 Medicine position stand. Progression models in resistance training for healthy adults," 2009; Morton, Colenso-Semple, & Phillips, 2019). Future
411 research is warranted to examine global strength capacity following ACL reconstruction to determine if stronger associations with
412 biomechanical variables during movement tasks are present. For detailed information regarding practical applications to return athletes to high
413 performance we recommend recently published articles (Buckthorpe, 2019; Buckthorpe & Della Villa, 2019; Maestroni, Read, Bishop, &
414 Turner, 2020; Welling, et al., 2019).

415 Our understanding of how residual deficits in power and RFD during single and multi-joint
416 movements and their relationships with kinetic and kinematic variables is limited and should
417 be the focus of future studies. Similarly, due to its association with stretch-shortening cycle
418 performance, relationships between reactive strength and biomechanical variables should also
419 be examined in athletic populations following ACL reconstruction. In addition, the
420 importance of monitoring contralateral limb capacity during rehabilitation (i.e.
421 concentric/eccentric strength, RFD and RSI) should not be underestimated due to the
422 potential for deconditioning which may increase injury risk and reduce an athlete's readiness
423 to re-perform.

424 When interpreting the conclusions of this review, it should be considered that we did not
425 perform a systematic review. Thus, a specific inclusion criteria was not applied and the level
426 of evidence, methodological quality and risk of bias in individual studies were not assessed in
427 this manuscript. The current narrative review provides a synthesis and critique of the
428 literature in this broad research area, and thus further opportunities for critical analysis.

429 **9.0 Conclusions**

430 This article examined the degree of association between fundamental physical qualities, such
431 as strength, rate of force development/power and reactive strength and biomechanical
432 variables during movement tasks in participants following ACL reconstruction. The available
433 data suggests that quadriceps strength and RTD, explain a moderate portion of the variance in
434 aberrant kinetic and kinematic strategies commonly detected in ACL reconstructed cohorts at
435 who are during the later stages of rehabilitation and RTS. The concepts expressed in this
436 article may help clinicians to optimise rehabilitation outcomes following and reduce re-injury
437 risk.

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